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Dynamics study of constant DI and constant TR control for cardiac alternans based on a two dimensional cellular automata model

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ABSTRACT

As a precursor for cardiac arrhythmias such as atrial and ventricular fibrillations, which could cause sudden cardiac death (SCD), cardiac alternans is essentially an unstable heart rhythm with alternating long and short action potential durations (APD) of cardiac myocytes that usually occurs under fast pacing conditions. In this paper, the constant TR control method based on global pseudo-electrocardiogram (ECG) is studied and compared with the local constant diastolic interval (DI) control method using a 2-dimensional (2-D) cellular automata model (CAM), aiming at preventing or eliminating cardiac alternans before arrhythmias. The results show that both the constant TR and constant DI control methods are effective in stabilizing the alternans to a smaller basic cycle length (BCL). Also, the efficacy of the two control approaches depends on the “decrease step” Δ in the downsweep protocol, and a smaller Δ could significantly improve their performance. Besides, in general, constant TR control is superior to constant DI control in alternans prevention when a relatively large Δ is adopted.

Keywords: Cardiac arrhythmias; alternans; conduction block; constant DI control; ECG; constant TR control; cellular automata model.

INTRODUCTION

Cardiac alternans is a disturbed heart rhythm in which the action potential duration (APD) of cells alternates between long and short values, and manifests on electrocardiograms (ECG) as alternation in amplitude between two consecutive T-waves ^[1]. In experimental and clinical practice, cardiac alternans could be a sensitive indicator of arrhythmias leading to life-threatening sudden cardiac death (SCD), which accounts for the death of around 325,000 Americans per

year. Thus, understanding and preventing cardiac alternans has been a research topic of great significance [2].

Based on the restitution theory, which has been widely used in cardiac alternans research, the APD of a cell in one cycle is a function of its diastolic interval (DI) in previous cycle, as shown in Eq. (1), where DI is the difference between the basic cycle length (BCL) and APD in the same cycle.

$$APD_{n+1} = f(DI_n) \quad (1)$$

where f is the restitution curve.

Then, as shown in Fig. 1(a), under a constant BCL or so-called periodical pacing protocol, when the BCL is long (e.g., $BCL=BCL_1$), the cardiac response is normal and APD is locked as 1:1 rhythm, and at steady state

$$\begin{aligned} APD_1 &= f(DI_1) \\ BCL_1 &= APD_1 + DI_1 \end{aligned} \quad (2)$$

Also, as shown in Fig. 1(b) and Fig. 1(c), APD alternates between APD_2 and APD_3 when $BCL=BCL_2$ is small and then we have:

$$\begin{aligned} APD_2 &= f(DI_2) \\ APD_3 &= f(DI_3) \\ BCL_2 &= APD_2 + DI_3 = APD_3 + DI_2 \end{aligned} \quad (3)$$

Besides, Eq. (1) indicates that alternans occurs when slope of the restitution curve is smaller than 1 [3],[4]. As shown in Fig. 1(c) and Fig. 1(d), APD alternates when BCL is smaller than BCL_{ONSET}^{BCL} , and stable normal response occurs when BCL is larger than BCL_{ONSET}^{BCL} , so BCL_{ONSET}^{BCL} is a bifurcation point.

To suppress cardiac alternans, different control methods have been proposed and tested in the past decades using both numerical models and/or experiments on isolated animal hearts. An adaptive proportional feedback control approach was proposed and tested on rabbit hearts in [4]. In [5], an alternating-period feedback control mechanism was tested through numerical simulation on a single cell and a 1-dimensional (1-D) tissue. Besides, the effect of a feedback control method was studied on isolated canine Purkinje fibers in [6]. However, feedback control methods are generally ineffective for tissue with a distance longer than 2 cm due to complex

spatiotemporal electrophysiological dynamics, and stimulation from multiple sites are required for large tissues, also, it is difficult to determine optimal control parameters ^{[7]-[9]}.

Due to the limited success of the feedback control, which utilises a beat-to-beat regulation of the BCL, a constant DI control method that decouples the relation between APD and DI was adopted to better suppress alternans ^[10]. As shown in Fig. 2, constant DI pacing protocol keeps the DI of the cell constant based on measured transmembrane voltage of the 1st cell in a tissue. In this way, the instability caused by change of APD can be eliminated, thus the pacing rhythm could be easier stabilized. Constant DI control was employed and tested in single-cell models ^{[10],[11]} and ventricular fibers models ^{[12],[13]} based on numerical simulation and/or experiments. However, these studies have validated efficacy of the constant DI control only on 0-D or 1-D tissues, and demonstrated that control may fail on 1-D cables and 2-D tissues with large size due to complex spatiotemporal evolution of cardiac activity ^{[14],[15]}. In addition, it is challenging to apply constant DI control in experiments due to the difficulty of performing real-time APD and DI measurements ^[15]. So, it is important to develop other control approaches with higher efficacy. As is known, the APD alternans can be observed on ECG as T-wave alternans which is easier to be detected in real-time ^{[16],[17]}, and the TR interval can be regarded as a global DI. Thus, similar to the concept of constant DI control, a constant TR control method was proposed and employed in recent research ^{[15],[17],[18]}. As shown in Fig. 3, under constant TR pacing, based on the ECG of the whole tissue, stimulations are added after detection of T peaks to keep TR intervals on the ECG constant, and therefore the constant TR protocol can be regarded as a “globalized” version of the constant DI protocol. In [15], the antiarrhythmic effects of constant TR control were validated using experiments on ex vivo whole rabbit hearts, yet there are some limitations such as accurate detection of a distinct T-wave and size of the heart. In [17], based on a 1-D numerical model of human ventricular tissue (<7 cm), the efficacy of constant TR control of alternans was studied and compared with that of constant DI control. The results show that the constant TR control is superior for alternans control in longer fibers when compared to constant DI pacing. Nevertheless, the simulation efficiency was low, and the study has not been performed on a higher dimensional (e.g., 2-D) model with a larger size.

Thus, it is of great significance to efficiently study cardiac alternans control on a high dimensional model with large sizes, and a cellular automata model (CAM) is a good choice to achieve this goal. As a powerful model, which has successful applications in biology, physics,

and other engineering areas, a CAM uses simple rules to compute complex phenomena with fewer calculations, and the process can be easily visualized to provide an intuitive illustration of system dynamics ^[19]. Although CAMs are less accurate than detailed models and vivo animal hearts experiments, they can represent the main features and key dynamical behaviors of the cardiac tissue. Compared with regular full physiological models, which require extensive computation, CAMs are much more efficient. Also, compared with ex vivo hearts, CAMs are more convenient and economical for tests on tissues of different sizes.

In this paper, we tested the efficacy of both the constant DI and constant TR control on alternans prevention using a 2-D CAM.

METHODS

Two-Dimensional CAM for Cardiac Simulation

Both 2-D and 3-D CAMs have been developed to simulate cardiac electrical wave propagation and fibrillation ^{[20]-[26]}; however, dynamical phenomena related to cardiac alternans have never been studied in these publications. Recently, a 2-D CAM capable of simulating cardiac dynamics including ectopic beat, wave break, spiral wave, conduction block, and alternans was proposed by our group ^[27]. Here, we adopted the same model with better practical parameter settings for the study of cardiac alternans control. Detailed mechanism of the employed 2-D CAM is described below.

Wave Propagation Rule in the CAM

To simulate dynamics of a 2-D cardiac tissue, an $n \times n$ CAM is constructed by MATLAB, and each small square in the CAM represents an individual cell of the tissue. Then, based on their transmembrane voltages, the cell states can be divided into four categories as listed in Table I ^[20], where the transmembrane voltage of a cell becomes 1 when it is excited or stimulated.

A 3×3 square, which contains 9 cells in the bottom left corner of the CAM, acts as the paced cells, and they excite according to some protocols such as periodic pacing. Besides, as shown in Fig. 4, a single cell (black square) is excited at next time step, if its transmembrane voltage is less than 0.1 V and the voltages of at least three adjacent cells (gray squares) are bigger than 0.9

V^[26]. Otherwise, its transmembrane voltage just evolves with time according to the voltage waveform function, which will be introduced below.

Transmembrane Voltage Waveform Function

The transmembrane voltage of a cell will suddenly change to 1.0 V the moment it is excited, otherwise, its voltage will progress according to the function below:

$$V(APD, t) = \frac{e^{-t/T(APD)}}{c + e^{-t/T(APD)}} \quad (4)$$

$$T(APD) = \frac{APD}{\ln(0.9) - \ln(0.1 \times c)} \quad (5)$$

where t is the time elapsed since last stimulation; c is a constant number which ensures $V(APD, t=0) \approx 1.0$ V and is set as 0.001 in this model; APD is determined by a restitution curve which will be given in next section. Thus, when the APD is determined, the parameter T can be calculated by Eq. (5), and then transmembrane voltage V in Eq.(4) will decrease from 1 to nearly 0 with the increase of t .

In addition, it can be easily proved or calculated that $V(APD, t=APD)=0.1$ V, which is exactly the refractory threshold. This also helps to define that the APD in this CAM is the time duration for the voltage to decrease from 1 V to refractory threshold 0.1 V.

For example, when $APD=300$ ms, the transmembrane voltage waveform given by Eq. (4)-(5) is shown in Fig. 5.

Restitution Curve

To provide the value of APD for calculation of transmembrane voltage in Eq. (4), the restitution curve used in this paper is given below according to cardiac restitution theory:

$$APD_{n+1} = f_{restitution}(DI_n) = 315 - 50e^{(70-DI_n)/50} \quad (6)$$

where the subscript $n+1$ and n denote the $(n+1)^{th}$ and n^{th} stimulation cycle, respectively.

From the restitution curve, it can be observed that APD_{n+1} increases with DI_n in a nonlinear way. In addition, the cardiac pacing is undatable when $d(APD_{n+1})/d(DI_n) > 1$, as illustrated in Fig. 1, which happens on the restitution curve determined by Eq. (6) when $DI < 70$, or $APD < 265$, and $BCL = APD + DI < 335$, as marked in Fig. 6.

With the CAM introduced above, cardiac scenarios such as periodic normal conduction, normal conduction considering scar tissue, spiral wave, and especially alternans can be simulated efficiently in MATLAB, and the case illustrations can be found in [27].

Pacing Protocols

Downsweep protocol is a widely used pacing method to study cardiac dynamics. Typically, pacing of the tissue starts from a long $BCL=BCL_0$ (around 1000 ms), and then BCL is progressively decreased (equivalent BCL is used for constant DI and constant TR pacing). For each specific BCL value, a certain number of stimulations (typically 50) are applied to reach steady state ^{[28][29]}.

Constant BCL downsweep pacing protocol

Under constant BCL downsweep pacing, the paced cells are stimulated each time after a constant period. Based on the simulation model introduced above, the values of BCL are set as a series of numbers decreasing from 350 ms to 300 ms as shown in Eq. (7).

$$\begin{aligned} BCL(k) &= 351 - k \\ k &= 1, 2, \dots, 51 \end{aligned} \quad (7)$$

For each specific constant BCL value in the series, 50 stimulations are applied to ensure the wave reaches steady state.

Constant DI downsweep pacing protocol

Unlike the constant BCL downsweep pacing protocol, under a constant DI downsweep pacing protocol, the paced cells are stimulated each time after a constant period (i.e., DI) from the instant when their transmembrane voltage drops to the refractory threshold 0.1 V, which is the threshold to distinguish between APD and DI intervals.

In this paper, to test the efficacy of constant DI control on the CAM, the values of DI in control are set as a series of numbers decreasing from 80 ms to 1 ms as shown below:

$$\begin{aligned} DI(k) &= 81 - k \\ k &= 1, 2, \dots, 80 \end{aligned} \quad (8)$$

For each specific constant DI value in the series, 50 stimulations are applied to test the control efficacy ^{[10][15]}.

Constant TR downsweep pacing protocol

Under a constant TR pacing protocol, the paced cells are stimulated each time after a constant period (i.e., TR) from the instant when a T-wave peak on ECG is detected. A peak detection algorithm from [30] is applied in our work to conduct online T-wave peak detection.

The values of TR in control are set as a series of numbers decreasing from 145 ms to 1 ms, as shown below:

$$\begin{aligned} TR(k) &= 146 - k \\ k &= 1, 2, \dots, 145 \end{aligned} \quad (9)$$

For each specific constant TR value in the series, 50 stimulations are applied to test the efficacy of the control ^[15].

To conduct constant TR pacing, a ECG of the tissue should be recorded. In our CAM-based tissue, with electrode A and electrode B placed out of the tissue (see Fig. 3), the pseudo-ECG can be calculated as:

$$ECG = \Phi_e(x_B, y_B) - \Phi_e(x_A, y_A) \quad (10)$$

where ∇ denotes gradient operation; (x_A, y_A) is the location of electrode A; (x_B, y_B) is the location of electrode B; and the transmembrane potential Φ_e can be obtained by:

$$\begin{aligned} \Phi_e(x_A, y_A) &= \int (-\nabla V) \mathbf{g}(\nabla(1/r_A)) dx dy \\ \Phi_e(x_B, y_B) &= \int (-\nabla V) \mathbf{g}(\nabla(1/r_B)) dx dy \end{aligned} \quad (11)$$

where the distances r_A and r_B in Eq. (11) are provided by:

$$\begin{aligned} r_A &= \left((x - x_A)^2 + (y - y_A)^2 \right)^{1/2} \\ r_B &= \left((x - x_B)^2 + (y - y_B)^2 \right)^{1/2} \end{aligned} \quad (12)$$

where (x, y) is the location of any cell in the tissue.

Pseudo-ECG takes the action potential of all cells in the tissue into consideration; thus, it is a global representation of cardiac dynamics ^[31].

SIMULATION RESULTS ON A 50×50 CAM

This section presents the simulation results under different pacing protocols using a 50×50 CAM. The central cell located at (25,25) is selected as a representative example to illustrate the pacing stability, and the straight diagonal cable from the paced cell at (0,0) to the corner cell at (50,50) is chosen to show the spatial dynamics. The simulation time step is 0.1 ms, and the threshold for alternans is set as 1 ms.

Cardiac dynamics under constant BCL downsweep pacing protocol

Firstly, under constant BCL pacing protocol, the bifurcation diagram of the central cell (25,25) under different BCL values and the spatial alternans along the diagonal cells at a constant BCL=320 ms are shown in Fig. 7.

It can be observed from Fig. 7(a) that alternans occurs at $BCL_{ONSET}^{BCL}=335$ ms, which is the same as the value calculated from the restitution curve in Eq. (6), and conduction block happens at $BCL_{CB}^{BCL}=311$ ms. Spatial concordant alternans (SCA) occurs along the diagonal cable as shown in Fig. 7(b) when BCL=320 ms, which also indicates SCA in the 2-D tissue.

Illustrations of normal response occurs at BCL=340 ms and alternans occurs at BCL=320 ms generated by a 200×200 CAM are shown in Fig. 8. From Fig.8 one can see that the waves have the same length (yellow color) under normal response but oscillate between small and large values under alternans.

Thus, the CAM provides an intuitive visual illustration of cardiac dynamics. Also, transmembrane voltage of the cell (25,25) under constant BCL=340 ms and BCL=320 ms are shown in Fig. 9.

From Fig. 9(a), we can also see that when BCL=340 ms, the APD remains constant, thus it is normal response. However, the APD under BCL=320 ms shown in Fig. 9(b) alternates.

Cardiac dynamics under constant DI downsweep pacing protocol

Secondly, under the constant DI pacing protocol, the results of the same central cell and diagonal cable as that in the constant BCL test are shown in Fig. 10. Here, the equivalent BCL is calculated by $f_{restitution}(DI)+DI$. Also, because $BCL=f_{restitution}(I)+I\approx 117$ ms when DI=1 ms, the limit of BCL under constant DI control pacing is given as $BCL_{LIMIT}^{DI}=117$ ms.

From the results in Fig. 10, there is no bifurcation, and the wave propagation can always be stable under constant DI protocol even when DI is 1 ms with a corresponding equivalent BCL less than 120 ms.

To better show the dynamic details, transmembrane voltage of cell (25,25) under constant DI=60 ms (equivalent BCL=314 ms), and DI=20 (equivalent BCL=199 ms), are shown in Fig. 11.

From Fig. 11, it can be observed that no matter under relative large or small equivalent BCL, e.g. under DI=60 ms or DI=20 ms, pacing of the cell (25,25) can always be stabilized.

Thus, simulation results validate the high efficacy of constant DI pacing on the 2-D CAM-based tissue.

Cardiac dynamics under constant TR downsweep pacing protocol

Thirdly, results under the constant TR pacing protocol are shown in Fig. 12. In the simulation, two electrodes are placed at (0,0) and (51,51) to generate the ECG.

From Fig. 12 we can see that the pacing is stable under constant TR pacing when TR is bigger than 26 ms with an equivalent BCL bigger than 117 ms. Also, conduction block occurs at $BCL_{CB}^{TR} = 117$ ms, and no alternans is observed in the whole process.

To illustrate detailed dynamics of the tissue under constant TR control, ECGs of the tissue and transmembrane voltage of the cell (25,25) under TR=118 ms (equivalent BCL=313 ms) and TR=61 ms (equivalent BCL=200 ms) are shown in Fig. 13 and Fig. 14, respectively.

From Fig. 13 and Fig. 14, no matter under relative large or small equivalent BCL, e.g. under TR=118 ms or TR=61 ms, both ECG of the tissue and pacing of the cell (25,25) can always be stabilized, which indicates normal response of the whole tissue.

Thus, the simulation results validate that constant TR control can achieve the same performance as constant DI control until conduction block happens, and $BCL_{CB}^{TR} = BCL_{LIMIT}^{DI}$.

DYNAMIC RESPONSE UNDER DIFFERENT DOWNSWEEP PROTOCOLS WITH DIFFERENT DECREASE STEPS FOR DIFFERENT MODEL SIZE

In the last section, the efficacy of both constant DI and constant TR approaches were validated on a 50×50 model using a downsweep protocol where the DI and TR decrease by 1 ms each step. The results show that both constant DI and constant TR control approaches could help to significantly decrease the equivalent BCL at which unstable dynamics occurs. More specifically, both approaches are fully effective in controlling alternans until an equivalent BCL is smaller than BCL_{LIMIT}^{DI} , which is the smallest BCL that can be given by restitution curve.

However, the results in [17] show that both constant DI and constant TR pacing protocols have limited effect on alternans prevention when a 5 ms decrease step is adopted in the downsweep protocol, and both alternans and conduction block will occur.

Thus, to fully study efficacy of the two control methods, in this section, dynamic responses of the system under the three pacing protocols, e.g. constant BCL, constant DI, and constant TR, using downsweep protocols with different decrease steps are studied along with a consideration of model size.

Firstly, downsweep protocols with different “decrease steps” Δ of 1 ms, 5 ms, and 10 ms are applied in constant BCL, constant DI, and constant TR pacing protocols, as shown in Eq. (13). For example, when $\Delta=5$ ms, we can get $DI(k)=(80-5(k-1))=85-5k=\{80,75,70,\dots,10,5\}$. Secondly, size of the square model was varied from 4×4 size to 50×50 size.

$$\begin{aligned}
 BCL(k) &= (350 - \Delta \cdot (k - 1)) \in [300, 350] \text{ ms} \\
 DI(k) &= (80 - \Delta \cdot (k - 1)) \in [1, 80] \text{ ms} \\
 TR(k) &= (145 - \Delta \cdot (k - 1)) \in [1, 145] \text{ ms} \\
 k &= 1, 2, 3, L \\
 \Delta &\in \{1, 5, 10\} \text{ ms}
 \end{aligned} \tag{13}$$

where Δ is the decrease step of downsweep protocols.

Performance of the three pacing protocols was tested and results are shown in Fig. 15-17.

From simulation results, system dynamics remain the same when the model size is bigger than 20×20, thus only performance on tissues with a size less than 20 is given in BCL_{ONSET} comparison. In addition, the BCL_{CB} does not change with model size and is plotted in the histogram.

From the results, it can be observed that:

(1) For constant BCL pacing protocol, the simulation results, including BCL_{ONSET} and BCL_{CB} remain the same independent of the model size and Δ .

(2) Both constant DI and constant TR pacing protocols are effective to prevent alternans compared with constant BCL pacing, and both protocols stabilize cardiac response till the minimum equivalent BCL, e.g. $BCL_{\text{LIMIT}}^{\text{DI}}$, for $\Delta=1$ ms. However, their efficacy decays with the increase of Δ in the downsweep protocol.

(3) For $\Delta>1$ ms, i.e. 5 ms and 10 ms, the constant TR control is generally more effective than constant DI control.

In comparison, paper [17] used a fixed decrease step $\Delta=5$ ms and presented that both constant DI and constant TR will cause alternans and conduction block when values of DI and TR are small. This is the same as what we observed in the CAM when decrease step Δ is set as 5 ms or 10 ms in the downsweep protocol. However, the effect of different decrease steps on control efficacy has not been studied and is first investigated in this paper. As observed from the numerical simulation, both constant DI and constant TR approaches are fully effective if the decrease step Δ in downsweep protocols are small enough.

CONCLUSION AND DISCUSSION

Based on a 2-D CAM, the efficacy of constant DI and constant TR pacing protocols on alternans prevention or elimination are studied in this paper by numerical simulation. Unlike the existing simulation work focusing on 0-D or 1-D tissue, the work in this paper is done on a 2-D model. Although less accurate than real heart experiments, CAM provides an economical and efficient approach for cardiac dynamic research and establishes a basis for both higher dimensional cardiac simulation and alternans prevention in heart tissue.

Simulation experiments in this paper validate that:

(1) CAM provides high efficiency and intuitive visual illustration for cardiac electrical wave propagation simulation.

(2) Both constant DI and constant TR protocols are effective to resolve cardiac alternans. However, their efficacy depends on the adopted decrease step in downsweep protocols, and a small decrease step could improve their performance.

In the meanwhile, there are some limitations of this study:

(1) The employed CAM uses simple rules to simulate wave propagation, and the accuracy is not as high as the traditional full physiological model. The rules can be improved to keep a better balance between efficiency and accuracy.

(2) The intracellular calcium cycling which is important for alternans development is not considered.

Future work can be done on the following aspects:

(1) Using a 3-D CAM to simulate cardiac wave propagation and study the efficacy of different control approaches.

(2) Improving the rules of CAM so that more details can be included without a significant sacrifice of computation efficiency.

(3) Study the essential mechanism in the dependence of control efficacy and decrease step in downswing protocols.

(4) Conduct tests on well-developed two-dimensional full physiological simulation models or *ex vivo* whole animal hearts to validate the results obtained from the CAM-based simulation in this paper.

CONFLICT OF INTEREST

The authors declare that they have no conflict of interest.

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DATA AVAILABILITY STATEMENT

The data that support the findings of this study are available from the corresponding author upon reasonable request.

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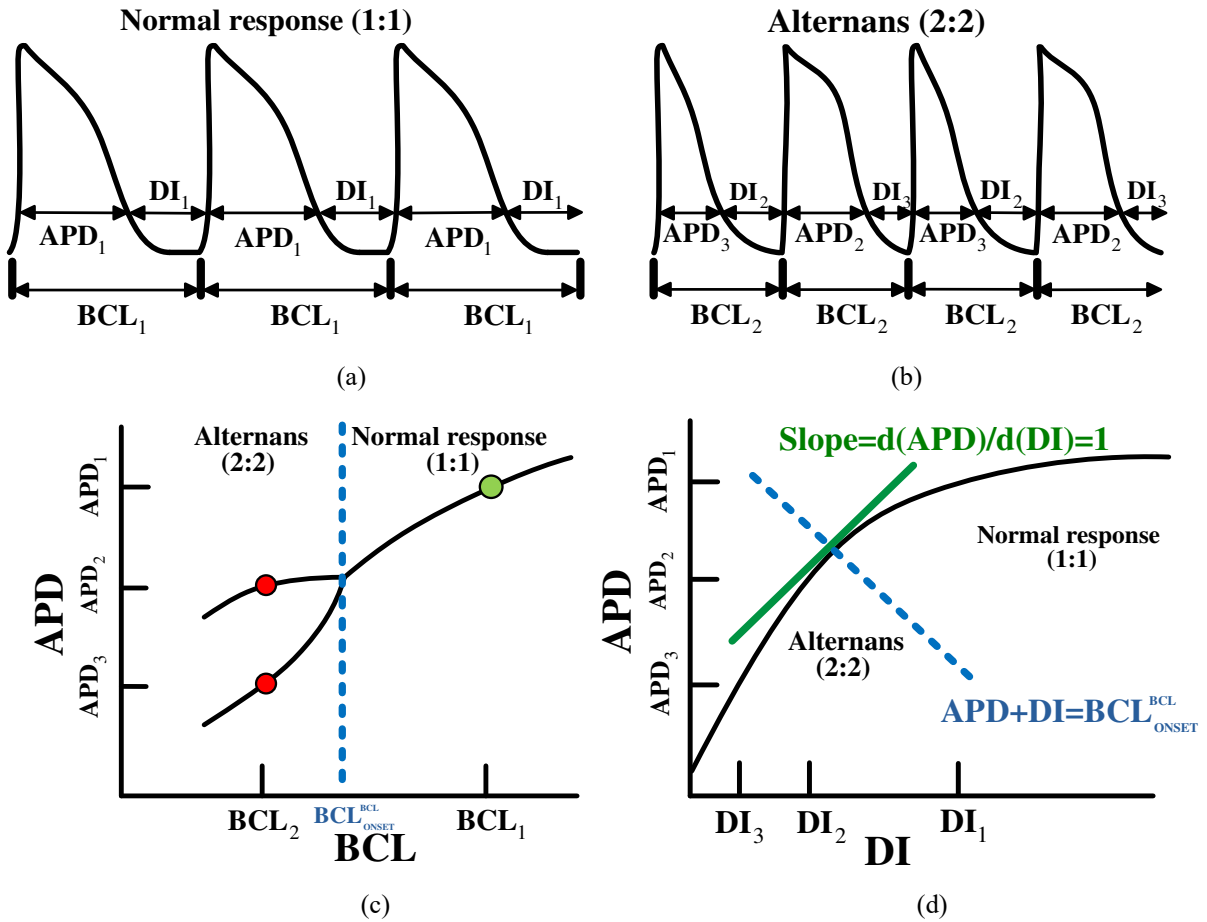


FIG. 1. Illustration of APD bifurcation under constant BCL pacing. (1) During normal response, APDs in each cycle remains the same. (2) During alternans, APD alternates between two different values. (3) Under constant BCL pacing, normal response occurs when $BCL \geq BCL_{ONSET}^{BCL}$ and alternans occurs when $BCL < BCL_{ONSET}^{BCL}$. (4) Under constant BCL pacing, at the point where slope of the restitution curve is 1, we have $APD + DI = BCL_{ONSET}^{BCL}$, and when the slope is bigger than 1, $APD + DI > BCL_{ONSET}^{BCL}$ and the pacing is normal, also, when slope is smaller than 1, then $APD + DI < BCL_{ONSET}^{BCL}$ and alternans occurs.

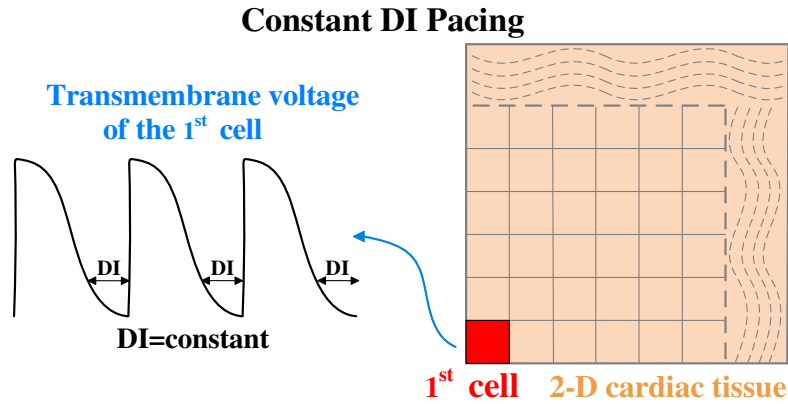


FIG. 2. Illustration of Constant DI pacing. In a 2-D tissue represented by the big yellow square, based on measured transmembrane voltage of the 1st cell which is marked in red, the tissue is paced after a preset duration when the transmembrane voltage drops below the threshold of DI.

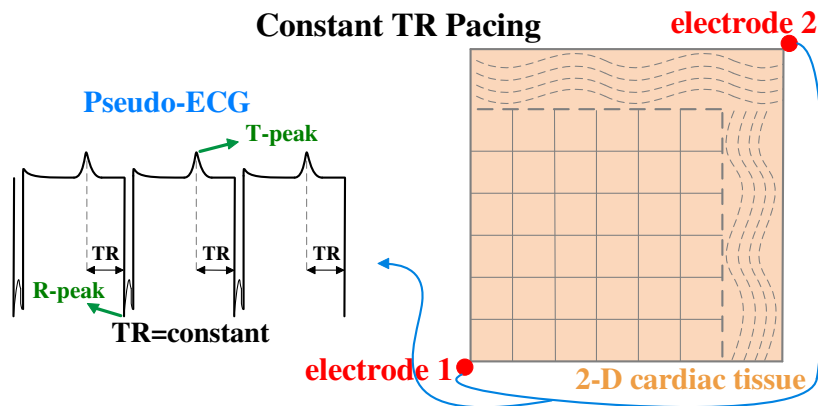


FIG. 3. Illustration of Constant TR pacing. In a 2-D tissue represented by the big yellow square, based on ECG of the whole tissue which is measured by two electrodes, the tissue is paced after a preset duration when the T-peak is detected.

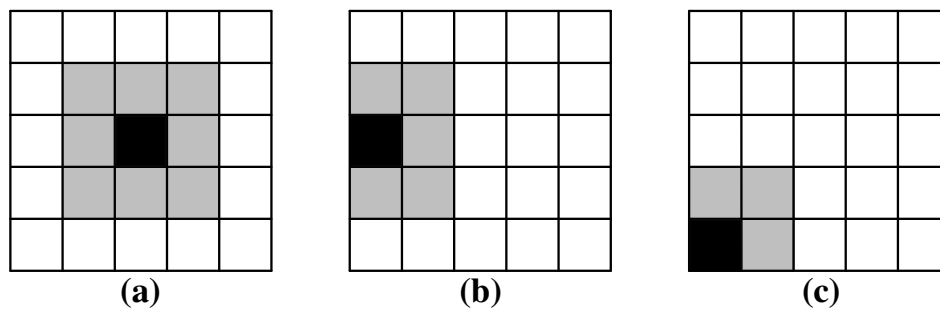


FIG. 4. Neighboring cells of a cell in a CAM. A black square represents any cell in the tissue, the gray squares are neighboring cells of the black cell. (a) A inner cell has eight neighboring cells. (b) A boundary cell has five neighboring cells. (c) A corner cell has three neighboring cells. During the wave propagation, to excite a black cell which is in relative refractory or resting state, at least three of its neighbors must be in excitation or absolute refractory state.

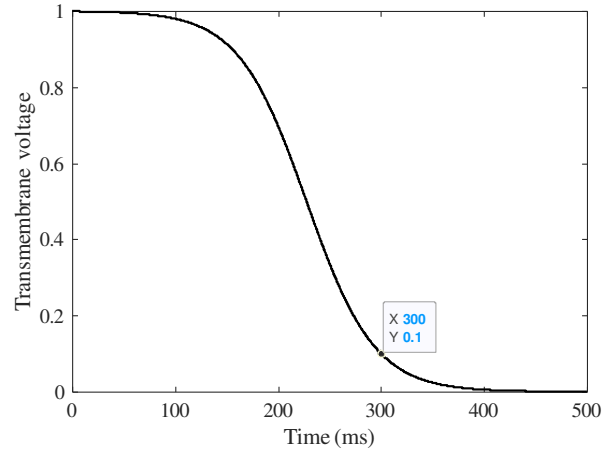


FIG. 5. Transmembrane voltage waveform when APD=300 ms. When a cell is excited, its transmembrane voltage becomes 1.0 V and then drops according to the voltage waveform. Its voltage will become 0.1 when the elapsed time is equal to APD=300ms.

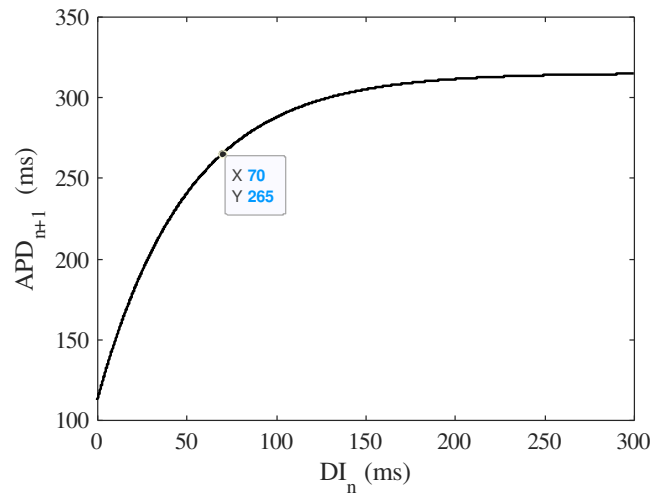


FIG. 6. Restitution curve in the CAM. The curve slope is 1 at the marked point (70,265). Thus, under constant BCL pacing, alternans occurs when $BCL < (70+265) \text{ ms} = 335 \text{ ms}$.

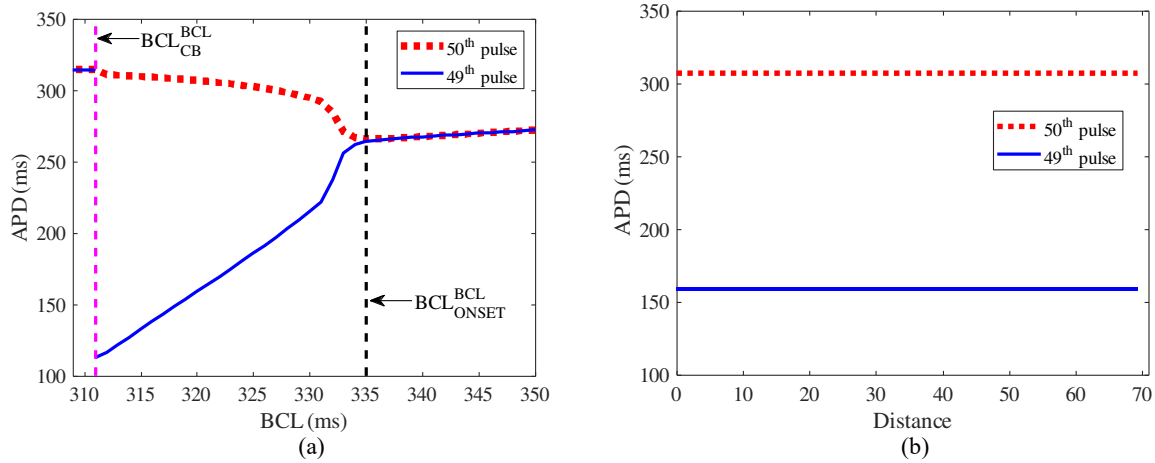


FIG. 7. Results of 2-D 50×50 model paced with constant BCL pacing protocol. (a) Bifurcation diagram at (25,25). $BCL_{ONSET}^{BCL} = 335$ ms is marker with vertical black dashed line; $BCL_{CB}^{BCL} = 311$ ms is marker with vertical pink dashed line. APD of cell (25,25) equals to 267.4 ms when $BCL = 340$, and alternans between 159 ms and 307 ms when $BCL = 320$ ms. (b) APD of the last two stimulation pulses along the straight diagonal cable from (1,1) to (50,50) at a $BCL = 320$ ms, where x axis is the distance of each cell to point (1,1), and alternans of APD between 159 ms and 307 ms can also be observed.

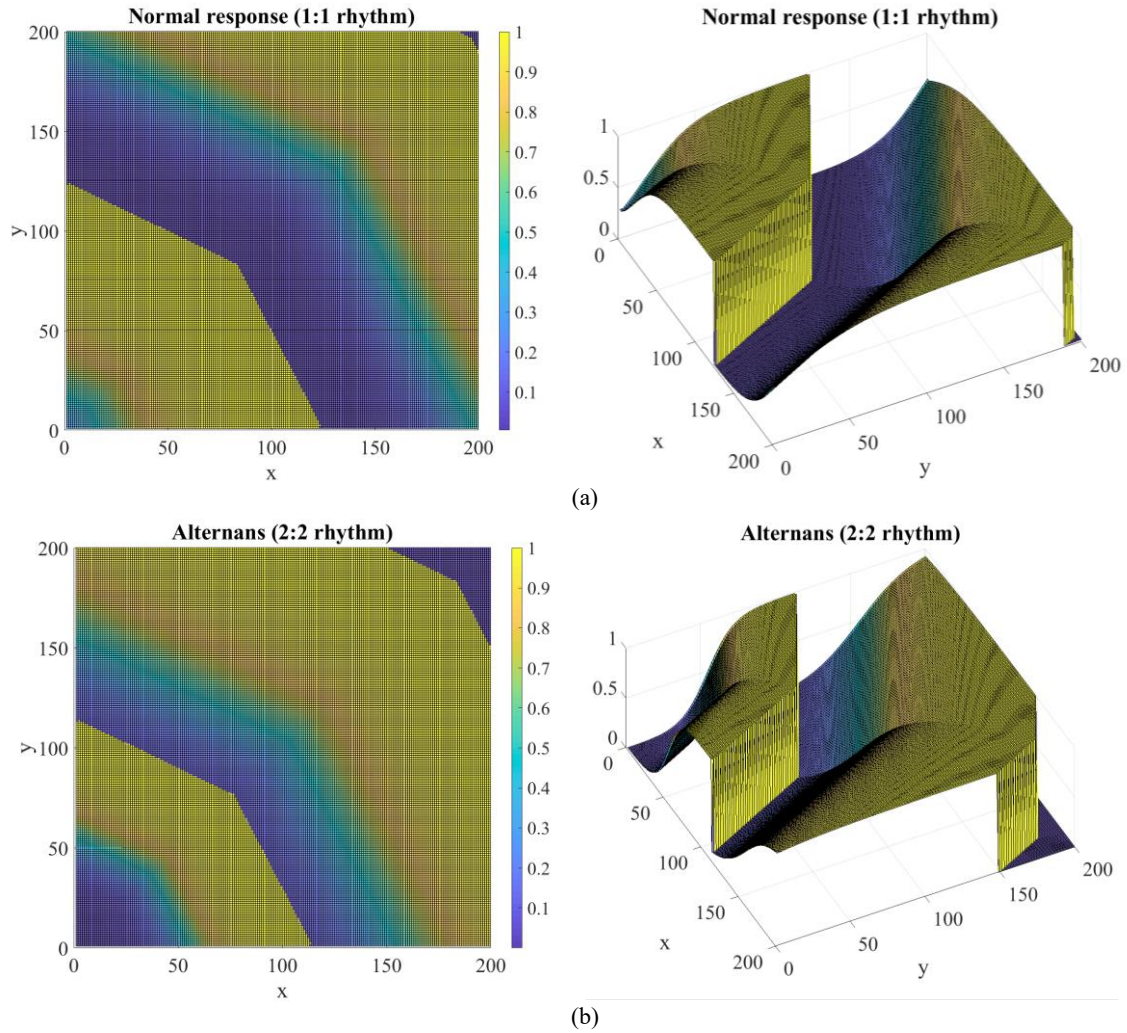


FIG. 8. Illustration of normal response and alternans in the CAM. Transmembrane voltage is represented by different colors as shown in the color bar. The left-hand-side pictures are in 2-D view and right-hand-side pictures are in 3-D view. (a) When $BCL=340\text{ms}$, caidiac waves have the same wave length and manifest 1:1 rhythm. (b) When $BCL=320\text{ms}$, caidiac waves have different wave lengths and manifest 2:2 rhythm.

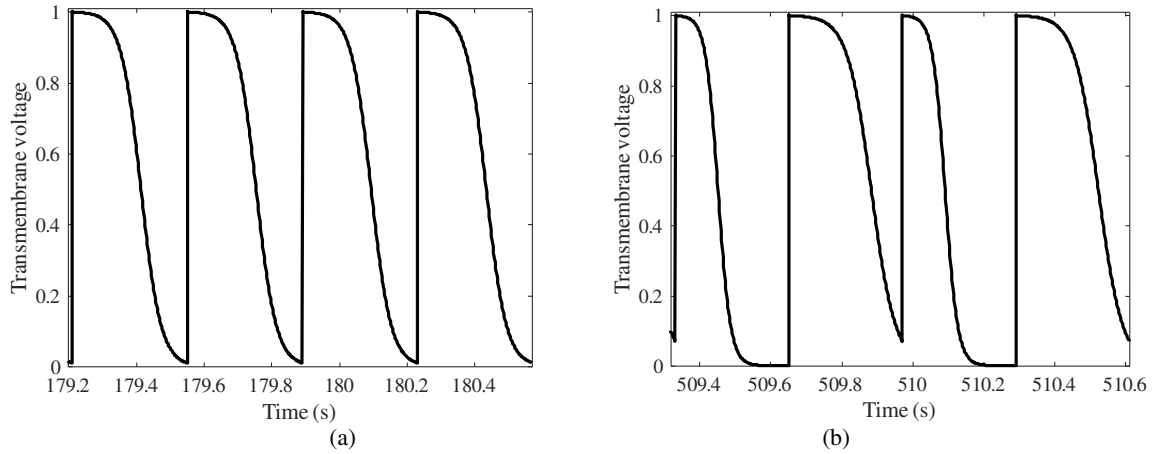


FIG. 9. Transmembrane voltage of cell (25,25) under constant BCL pacing protocol. (a) When BCL=340 ms, APD of the cell (25,25) is constant. (b) When BCL=320 ms, APD of the cell (25,25) alternates.

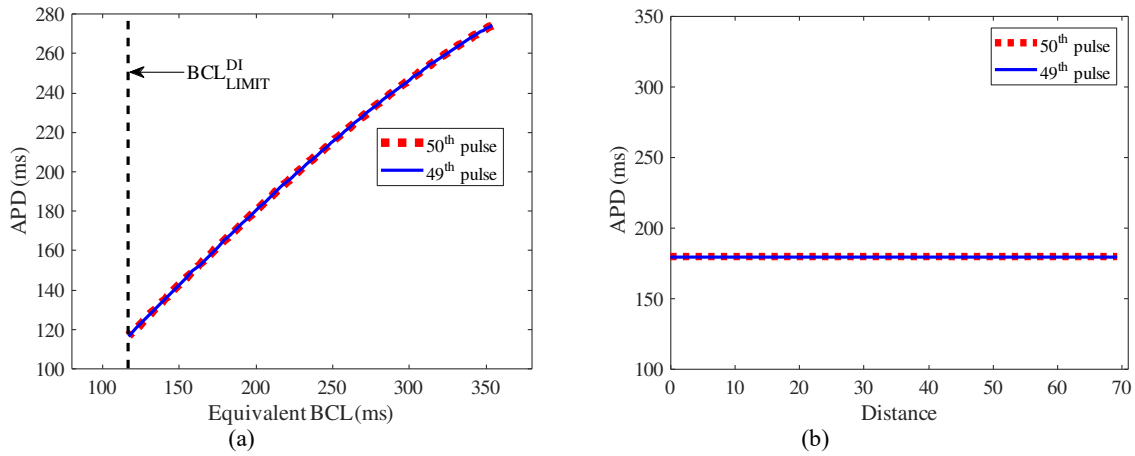


FIG. 10. Results of 2-D 50x50 model paced with constant DI protocol. (a) Bifurcation diagram at cell (25,25). $BCL_{LIMIT}^{DI} = 117$ ms is marker with vertical black dashed line. The pacing maintains as 1:1 rhythm under constant DI control. (b) APD of the last two stimulation pulses along the straight diagonal cable from (1,1) to (50,50) at DI=20 ms, where x axis is the distance of each diagonal cell to point (1,1).

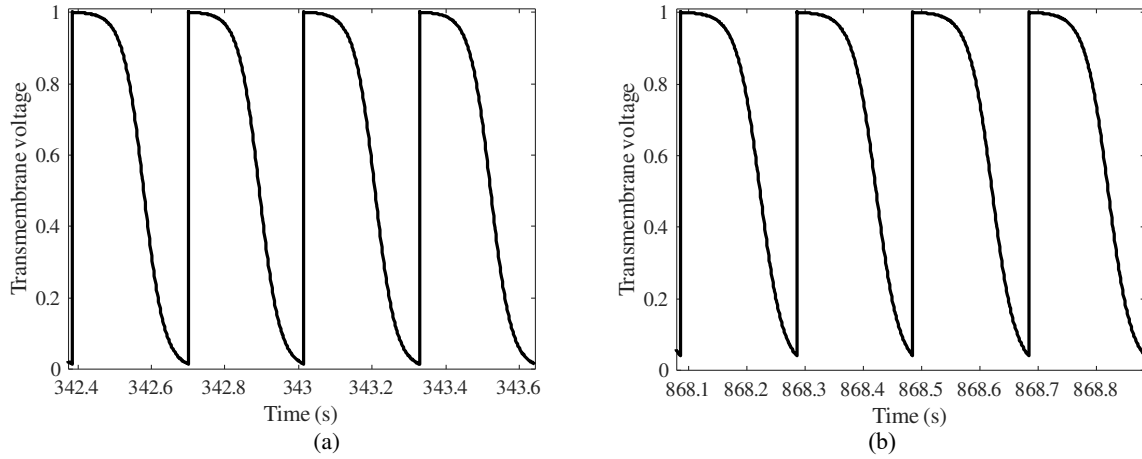


FIG. 11. Transmembrane voltage of cell (25,25) under constant DI pacing protocol. (a) When $DI=60$ ms, the equivalent BCL is 314 ms, and APD of the cell (25,25) remains constant. (b) When $DI=20$ ms, the equivalent BCL is 199 ms, and APD of the cell (25,25) also remains constant.

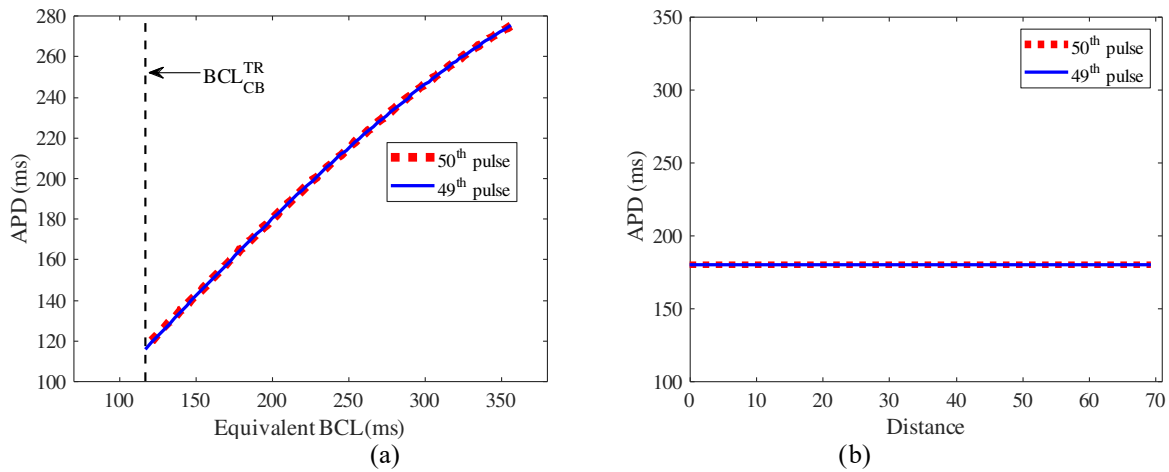


FIG. 12. Results of 2-D 50×50 model paced with constant TR protocol. (a) Bifurcation diagram at cell (25,25). $BCL_{CB}^{TR}=117$ ms is marker with vertical black dashed line. The pacing maintains as 1:1 rhythm under constant TR control until reaching BCL_{CB}^{TR} . (b) APD of the last two stimulation pulses along the straight diagonal cable from (1,1) to (50,50) at $TR=61$ ms, where x axis is the distance of each diagonal cell to point (1,1).

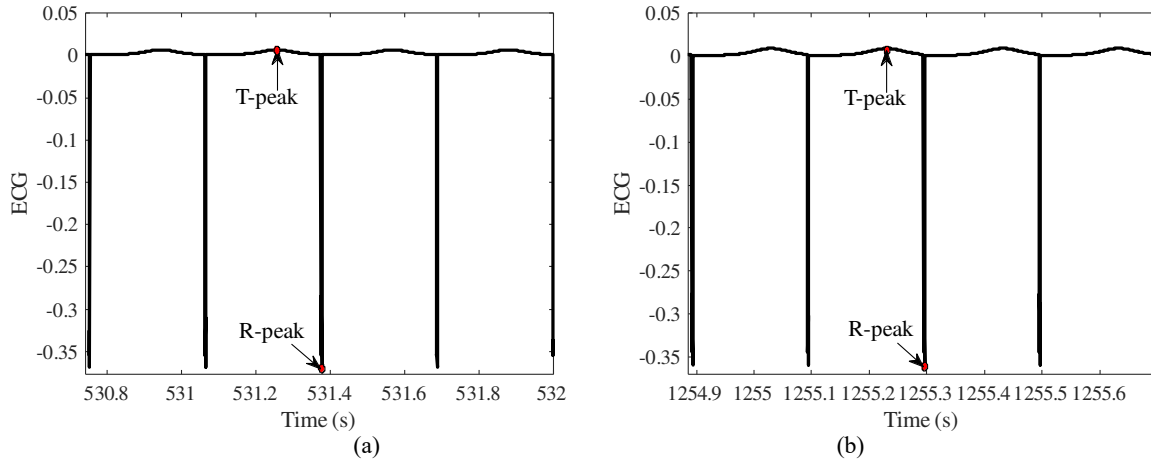


FIG. 13. ECG of the tissue under constant TR pacing protocol. T-peaks and R-peaks are marked as red points. ECG of every cycle having the same shape indicates 1:1 pacing rhythm. (a) When TR=118 ms, the equivalent BCL is 313 ms, and the pacing is stable. (b) When TR=61 ms, the equivalent BCL is 200 ms, and the pacing is also stable.

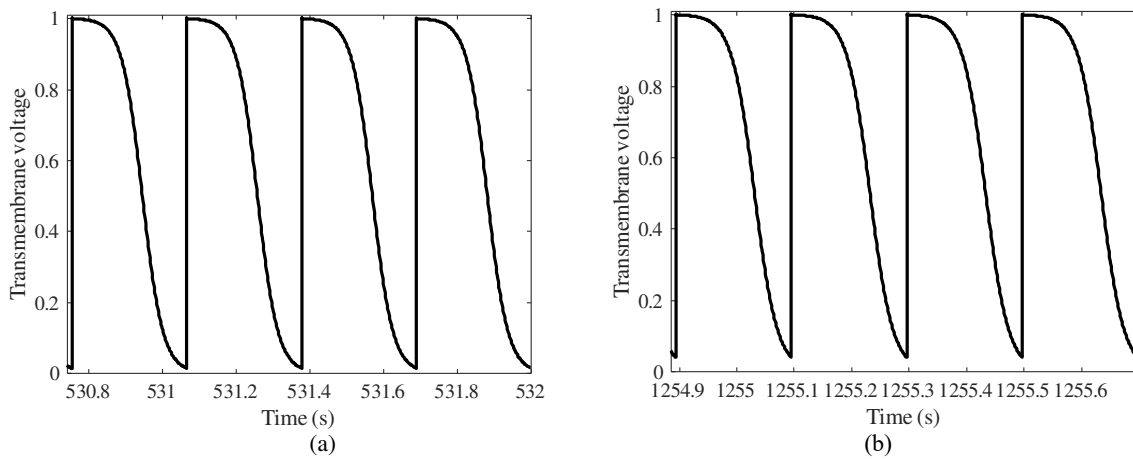


FIG. 14. Transmembrane voltage of cell (25,25) under constant TR pacing protocol. (a) When TR=118 ms, APD of the cell (25,25) remains constant. (b) When TR=61 ms, APD of the cell (25,25) also remains constant.

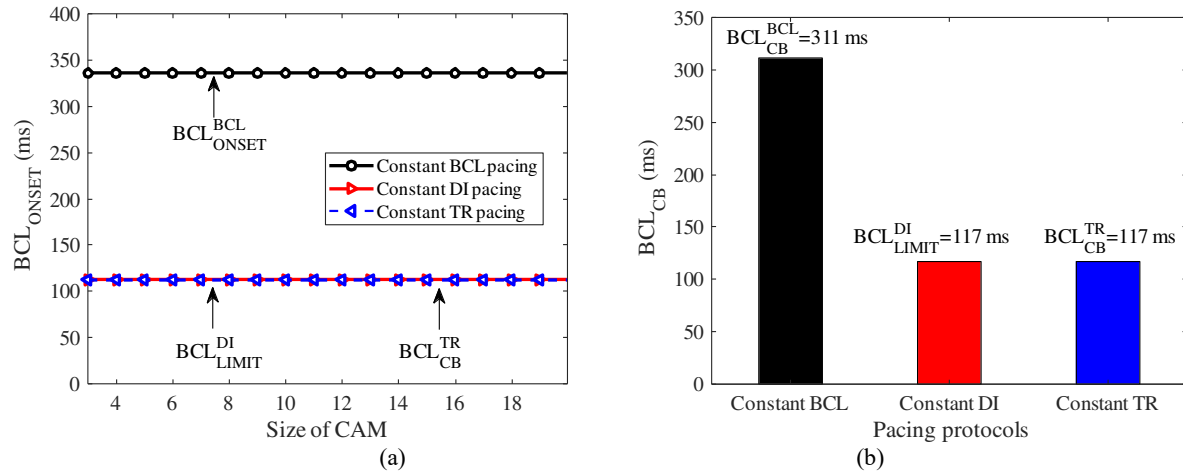


FIG. 15. Efficacy of different pacing protocols using downsweep protocols with a decrease step $\Delta = 1$ ms. (a) Results of BCL_{ONSET} under the three pacing protocols as a function of model size. The constant DI pacing protocol is fully effective till the corresponding equivalent BCL is smaller than BCL_{LIMIT}^{DI} . The constant TR pacing protocol can eliminate alternans till conduction block occurs at BCL_{CB}^{TR} . (b) Results of BCL_{CB} under the three pacing protocols.

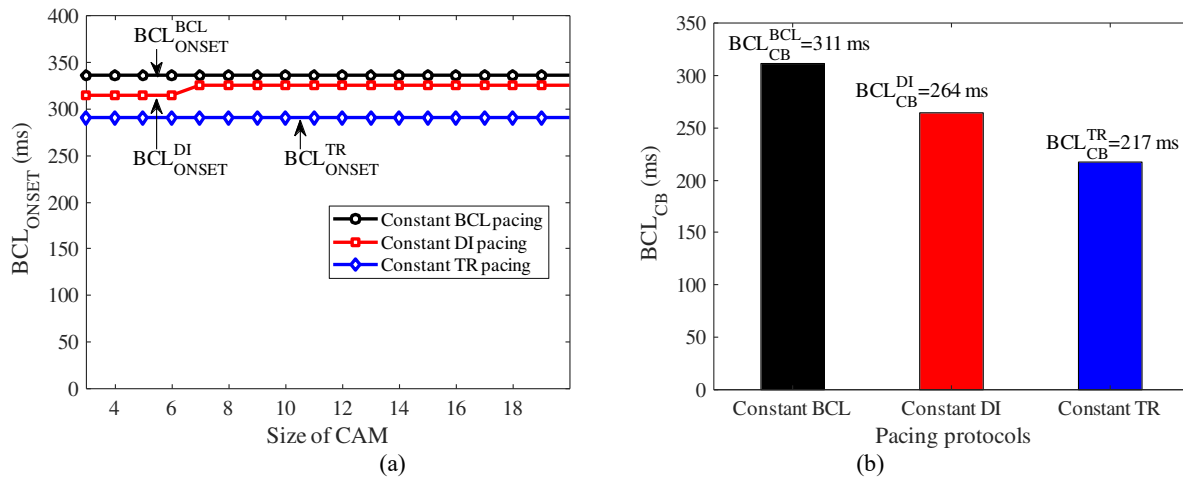


FIG. 16. Efficacy of different pacing protocols using downsweep protocols with a decrease step $\Delta = 5$ ms. (a) Results of BCL_{ONSET} under the three pacing protocols as a function of model size. (b) Results of BCL_{CB} under the three pacing protocols.

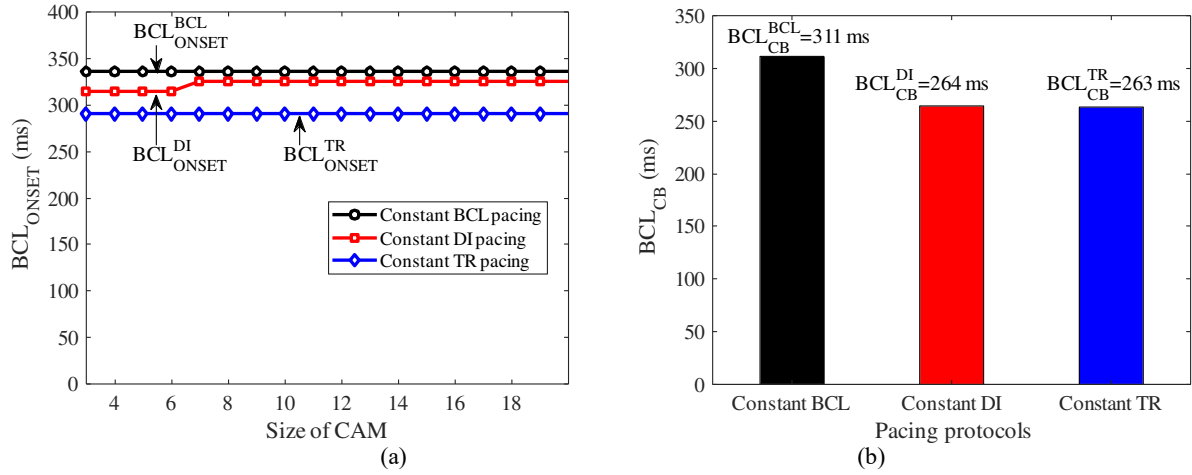


FIG. 17. Efficacy of different pacing protocols using downswEEP protocols with a decrease step $\Delta = 10$ ms. (a) Results of BCL_{ONSET} under the three pacing protocols as a function of model size. (b) Results of BCL_{CB} under the three pacing protocols.

Table I: States of cells

State	Action potential value	Characteristics
Excitation	[0.9, 1.0] V	Able to excite its neighbors, cannot be stimulated
Absolute refractory	[0.1, 0.9] V	Unable to excite its neighbors, cannot be stimulated
Relative refractory	(0, 0.1) V	Unable to excite its neighbors, can be stimulated
Resting	0 V	